

Research Article**Nasal delivery of Salbutamol loaded mucoadhesive microsphere for effective management of asthma**Vineeta Shyam¹, Kapil Khatri¹, Satish Shilpi^{1*}¹Pharmaceutical research laboratory, Department of Pharmaceutics, Ravishankar College of Pharmacy, Bypass Road, Bhanpur Square, Bhopal (MP)India

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Abstract

Objective: Salbutamol is a medication that opens up the medium and large airways in the lungs and it is used to treat asthma, exercise-induced bronchospasm, and chronic obstructive pulmonary disease (COPD). The objective of this dissertation work was to prepare salbutamol loaded microspheres using carbopol, **Materials and methods:** HPMC and sodium CMC for the purpose of effective management of asthma by delivering drug for long period of time in a controlled manner by making them mucoadhesive. Microspheres prepare by emulsification-heat stabilizing method and characterize on the basis of size, shape and surface morphology, drug content and drug release. **Results:** Microspheres were spherical shape and smooth in surface confirmed by scanning electron microscopy (SEM). The average size was found to be $12.14 \pm 2.53 \mu\text{m}$ and drug content was $80.15 \pm 1.02\%$. An in-vitro drug release study was revealed that microsphere release $52.16 \pm 1.76\%$ drug in 24 hr. **Conclusion:** It is concluded that prepared microspheres of salbutamol can be prepared by emulsification heat stabilizing method for high drug encapsulation and controlled drug release.

Keywords: Salbutamol, Microspheres, HPMC, Sodium CMC, Drug release

Introduction

Controlled release technology as rapidly emerged over the past three decades, as a new inter disciplinary science that offers novel approaches to the bioactive agents. Controlled drug delivery design involves the application of physical and polymer chemistry to dosage form design, to produces a well characterized and reproducible drug delivery profile (Celebi et al., 1996; Amperiadou et al., 1995; Cook et al., 2005). If drug targeting and retention time is increase in the target environment then controlled release delivery systems can achieve optimum therapeutic responses, prolong efficacy and decreased toxicity¹ (Cevik et al., 2000; Fu et al., 2002; Desai and Park, 2005; Young et al., 2006). It is possible, if drug delivery system provide a therapeutic amount of drug to the target sight in the body. The drug delivery system should

deliver drug at a rate detected by the needs of the body over the entire period of treatment (Khar et al., 2009; Chourasia et al., 2004).

Asthma is a common long term inflammatory disease of the airways of the lungs. It is characterized by variable and recurring symptoms, reversible airflow obstruction, and bronchospasm. Asthma is thought to be caused by a combination of genetic and environmental factors (Murthy and Hiremath, 2001; Martinez et al., 2007). Environmental factors include exposure to air pollution and allergens. There is no cure for asthma but symptoms may be controlled with effective asthma treatment and management. Symptoms can be also be prevented by avoiding allergens and irritants or by use of inhaled corticosteroids. Long-acting beta agonists (LABA) or antileukotriene agents may be used in addition to inhaled corticosteroids if asthma symptoms remain uncontrolled. Treatment of rapidly worsening symptoms is usually with an inhaled short-acting beta-2 agonist such as salbutamol and corticosteroids taken by mouth (Martinez et al., 2007). Salbutamol is adrenergic bronchodilators. It is generally administered by breath through the mouth to open up the air

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passages in the lungs. It is used to treat or prevent bronchospasm in patients with asthma, bronchitis, emphysema, and other lung associate complication. This medicine is also used to prevent exercise-induced bronchospasm (wheezing). But its high dosing frequency and side effect make it a suitable candidate to formulate in the form sustained release drug delivery system (Pachua et al., 2008; Prabakaran et al., 2004).

In this project, salbutamol laded polymeric microspheres is prepared which will administered by nasal route to lung. It mocoadhesiveness will help it to adhere with mucus layer of lungs tissue and release drug (salbutamol) in a sustained and controlled manner which will effectively manage the asthma for longer period of time. The mucoadhesiveness of microsphere will further increase it retention and making it available for drug release for longer period at the site of action.

Materials and methods

Materials

Salbutamol was obtained as gift sample from Cadila Pharmaceutical Laboratory Pvt Ltd, Ahmedabad, Gujrat, Indai. HPMC, Sodium carboxymethyl cellulose; tween-80 and span-80, cellophane dialysis tube MWCO 12000 were also purchased from Himedia Laboratories Pvt. Ltd, India. All other solvents used in the study were of HPLC grade and triple distilled water was used wherever required.

Preparation of salbutamol loaded microsphere

Microspheres of Salbutamol was prepared by emulsification solvent evaporation method (Chourasia et al., 2004; Amperiadou et al., 1995) with slide modification, in which carbopol, HPMC and sodium CMC were taken in different ration (2:1:1, 4:1:1, 6:1:1) and dissolved in 20 ml of deionised water with continuously stirring on mechanical stirrer. In this solution 0.1% w/v of Tween-80 was added and stirred continuously for 30 min. Drug (10% w/w of polymer) was added in polymer solution In another container 50mL of castor oil was taken with 1% w/v of span-80 and stirred it for 20 min. on mechanical stirrer. In this oil phase polymer solution was added drop wise with continuously stirring at 3000 rpm to form w/o emulsion. After 15 min 0.75mL of GST solution was added as cross linking agent and stirred the emulsion for 4 hr to evaporate water from internal phase and got suspension of polymeric microsphere. The suspension containing the micro-spheres was centrifuged for 5 min at 4000 rpm and the settled microspheres were washed three times with petroleum ether to remove oil from microspheres surfaces. Microspheres were again washed two times with acetone and then pour in Petridis to dry microsphere upon evaporating acetone. Dried microsphere stored in closed vessel until further use.

Characterization of microspheres

Determination of % yield of microspheres

Percent yield of prepared microsphere was determined by taking dried microspheres and weighed accurately. The percentage yield was then calculated using formula given below:

$$\% \text{ Yield} = \frac{\text{Mass of microsphere obtained}}{\text{Total weight of drug and polymers}} \times 100$$

Shape and Surface Morphology

The shape and surface morphology of prepared microsphere were visualized by scanning electron microscopy at AIIMS, New Delhi. Transmission electron microscopy (TEM, Morgagni 268 electron microscope) was used for visualizing particulate shape. Scanning electron microscopy (SEM) (Leo 435 VP, Cambridge, U.K., electron microscope) was also used to characterize the surface morphology of the microsphere. The dried microsphere on a double adhesive tape which was stuck to an aluminum stub and then coated with gold. The sample was then randomly scanned and photographs were taken (Figure 1a & b).

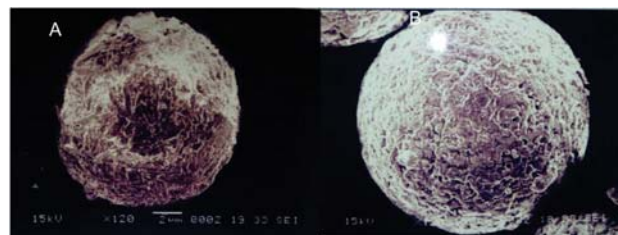


Figure 1. SEM photomicrograph of microsphere (a) without drug loaded (b) drug loaded

Particle Size and Zeta Potential

The size and size distribution analysis of Microsphere was done using Dynamic Light Scattering (DLS) technique using a computerized Malvern zetasizer (DTS ver. 4.10, Malvern instrument, England). Particulate suspension was mixed with the appropriate medium (1:100 dilution using double-distilled water) for particle size measurement. Zeta potential of microsphere dispersion was measured by Malvern zetasizer. Microsphere dispersion was put into the sample cuvette and the particle size was recorded.

Percent Drug Entrapment

Prepared microspheres were further characterized for entrapment efficiency. In this method 50mg of microsphere was taken in a beaker containing 5.0 mL of phosphate buffer pH 7.4 and stored at room temperature for 24 hr to leach out drug from microsphere. Then microspheres were crushed by pestle and mortar to extract out complete drug from microsphere matrix. Solution was centrifuged for 15 min at 3000 rpm and 1.0 mL of supernatant was taken diluted upto

10 mL and analyzes the sample using UV spectrophotometer.

$$\% \text{Entrapment Efficiency} = \frac{\text{Amount of drug in microsphere}}{\text{Total amount of drug taken}} \times 100$$

Invitro release studies

In vitro drug release from microsphere was carried out by using dialysis sac method. In which microspheres equivalent to 100 mg of drug were weighed and transferred into cellophane membrane tubing MWCO 12000 Dalton (Himedia) containing 5.0 mL of phosphate buffer pH 7.4. This sac was transferred in a beaker containing 100 mL of same phosphate buffer pH 7.4. Flask was kept on the magnetic stirrer and the media continuously at 100 rpm and temperature was maintained at $37 \pm 0.5^\circ\text{C}$. Then 1.0 mL of sample was withdrawn at suitable time interval using a hypodermic syringe attached with $0.45 \mu\text{m}$ membrane filter. Same volume of medium was replaced by phosphate buffer pH 7.4. After suitable dilution samples were analyzed on UV spectroscopy at 276 nm.

Results and discussion

Preparation and Characterization of microspheres

The Microspheres were prepared using emulsification solvent evaporation method. HPMC, Sodium CMC and carbopol were used as a polymer blend to form microsphere. The microspheres were stabilized with the non-ionic surfactants Tween 80 and span-80. The composition of the microsphere significantly affects the physicochemical properties and drug release profiles of Microsphere. The studies of various microspheres consisting of different ratios of HPMC, Sodium CMC and carbopol describe the effect of these variables on the size, and drug entrapment (Table 1). At lower level of HPMC, Sodium CMC, the size was found to be less but particles were of irregular shape and on increasing the same the particle size increases and there is increase in uniformity and entrapment efficiency, but on further increasing the ratio of HPMC, Sodium CMC the size increases abruptly. The formulation F2 was found to be optimum with respect to various parameters as discussed earlier.

Shape and surface morphology

Shape and surface morphology are very critical factor when designing such novel formulation as these are responsible for the

structural integrity and stability of the formulation. Surface morphology of the formulation was determined using SEM respectively as shown in figure 1a and b for without drug loaded and salbutamol loaded microsphere respectively. All the microsphere were found to be spherical with somewhat smooth in surface.

Particle size and zeta potential

To develop such controlled-release formulations particle size and Zeta potential are important parameter for stability of the formulation. Particle sizes and surface charges of the developed microsphere are shown in table 1. It was observed that the size of the optimized microsphere formulation was 12.14 ± 2.53 , which was optimum, when prepared with 1% surfactant (Tween 80). As depicted in table 1, the particle size of optimized microsphere when prepared with 4:1:1 ratio Carbopol: HPMC: NaCMC respectively was found to be $12.14 \pm 2.53 \mu\text{m}$ and zeta potentials of the microsphere was $20.45 \pm 0.28 \text{ mV}$. On increasing the concentration of Carbopol, i.e. 6:1:1 ratio of Carbopol: HPMC: NaCMC, particle size was increase.

Percent Drug Entrapment

The percent drug entrapment is an essential requirement for the fabrication of any drug delivery system. The results obtained in this study of salbutamol loaded Microsphere are shown in the table 1, which confirms good entrapment efficiency ($80.15 \pm 1.02\%$) of optimized microsphere (F2). On increasing the ratio of carbopol, entrapment efficiency was increase but size of microsphere also increases.

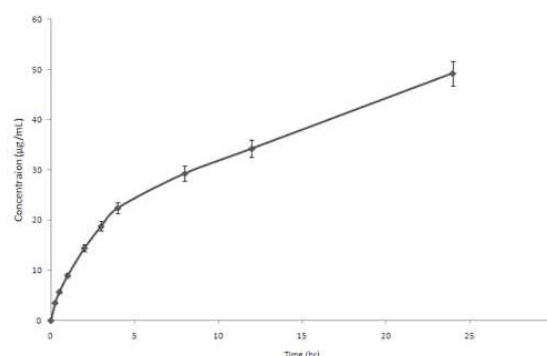


Figure 2. Cumulative percent drug release from salbutamol loaded microsphere

Table 1. Optimization of salbutamol loaded microsphere

Formulation code	Polymer Ratio Carbopol:HPMC:NaCMC	Drug (%) w/w	% Yield	Average Size (μm)	Entrapment Efficiency (%)	Zeta Potential
F1	2:1:1	10	84.22 ± 2.43	08.46 ± 3.22	72.63 ± 1.88	12.31 ± 0.42
F2	4:1:1	10	88.26 ± 3.09	12.14 ± 2.53	80.15 ± 1.02	20.45 ± 0.28
F3	6:1:1	10	85.52 ± 1.68	38.86 ± 2.86	81.54 ± 2.44	21.10 ± 0.56

In vitro drug release study

In order to estimate potential of the microsphere based gel formulation to retard the release of drug, it is necessary to calculate controlled release profile of the drug from the microsphere. The slow release profile may be the indicator of the temporal efficiency of the formulation. The release profile of salbutamol from microsphere formulations at different time interval are shown in the figure 2, shows $52.16 \pm 1.76\%$ in 24 h.

Conclusion

The microspheres of polymer blend (HPMC, sodium CMC and carbopol) were successfully prepared using emulsification solvent evaporation method in which salbutamol was loaded with high loading efficiency. Electron microscopy indicated that the salbutamol loaded microspheres were spherical in shape and smooth in surface. Size and zeta potential result shows that microsphere obtained by this method is in suitable in size and zeta potential represent good stability. The enhanced accumulation of salbutamol via microsphere and release drug well-controlled and sustained manner which will beneficial to manage asthma for longer period of time. The results obtained in this study reveal the merits of developed salbutamol loaded microsphere and justify their potential in strengthening the efficacy and safety of the drug as compared to existing conventional formulations in terms of lungs tolerability by patients. It is concluded that the prepared salbutamol loaded microsphere is a potential tool to deliver drug via nasal route for effective management of asthma.

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